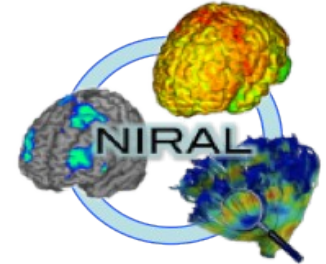




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Resampling Diffusion Tensor Images

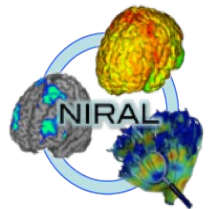
François Budin

Neuro Image Research and Analysis Laboratories



Overview

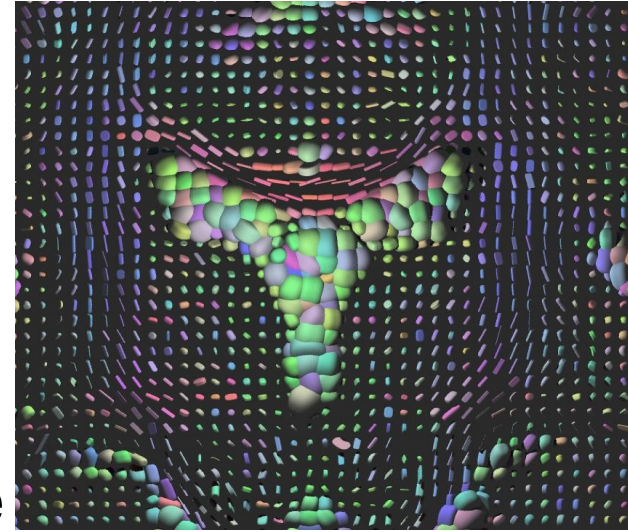
- Diffusion Tensor Images
- Resampling
 - Transformation
 - Interpolation
 - Structure preservation
- Results
- Conclusion





Diffusion Tensor Images

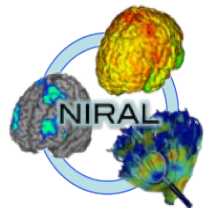
- Computed from a Diffusion Weighted Image (DWI)
- Represents the diffusion of water molecules in the brain
- Allows to visualize the structure of the tissues
- Each pixel contains a positive semi-definite symmetric matrix.
- Can be represented as an ellipsoid or a superquadric
 - The eigenvectors represent the orientation of the shape
 - The eigenvalues represent the size along each axis



Resampling: Why?



- Modify the property of the image:
 - Size
 - Orientation
 - Spacing
- Allows for the comparison between 2 images which are not initially aligned



Resampling: How ?



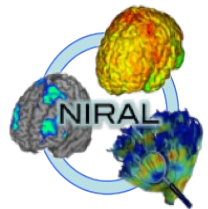
Can be separated in 2 steps:

– Transformation

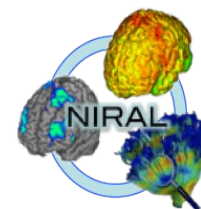
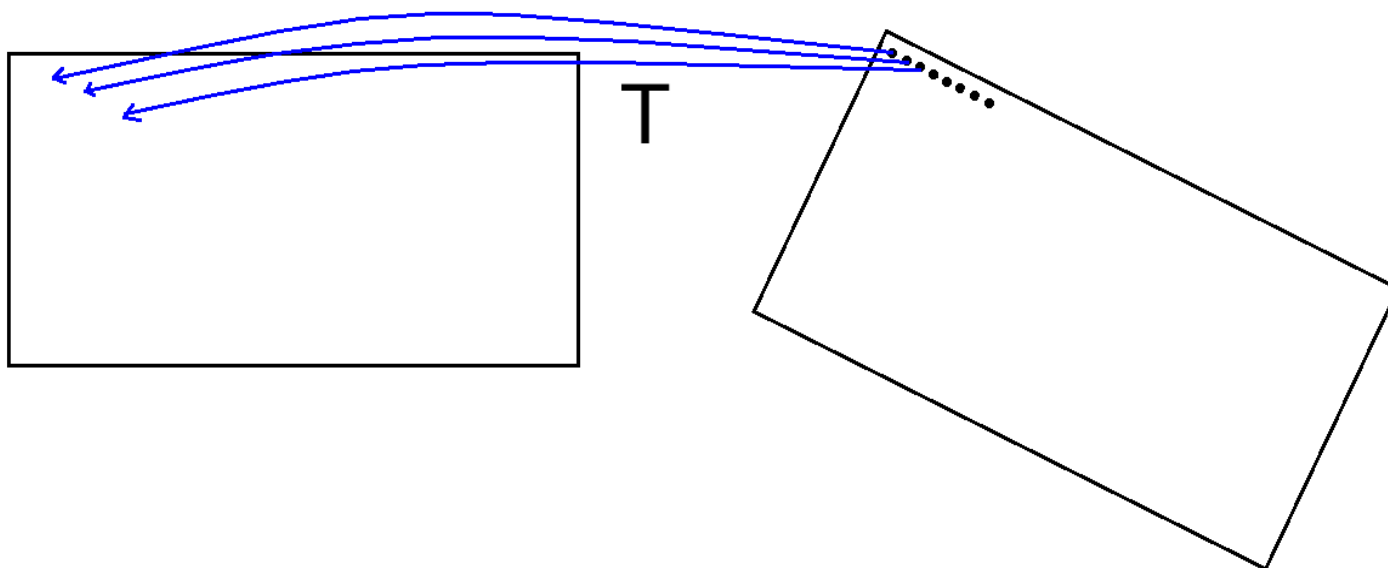
- Translation
- Rotation
- Affine transformation
- Non-rigid transformation

– Interpolation

- Nearest Neighbor
- Linear

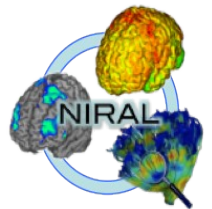
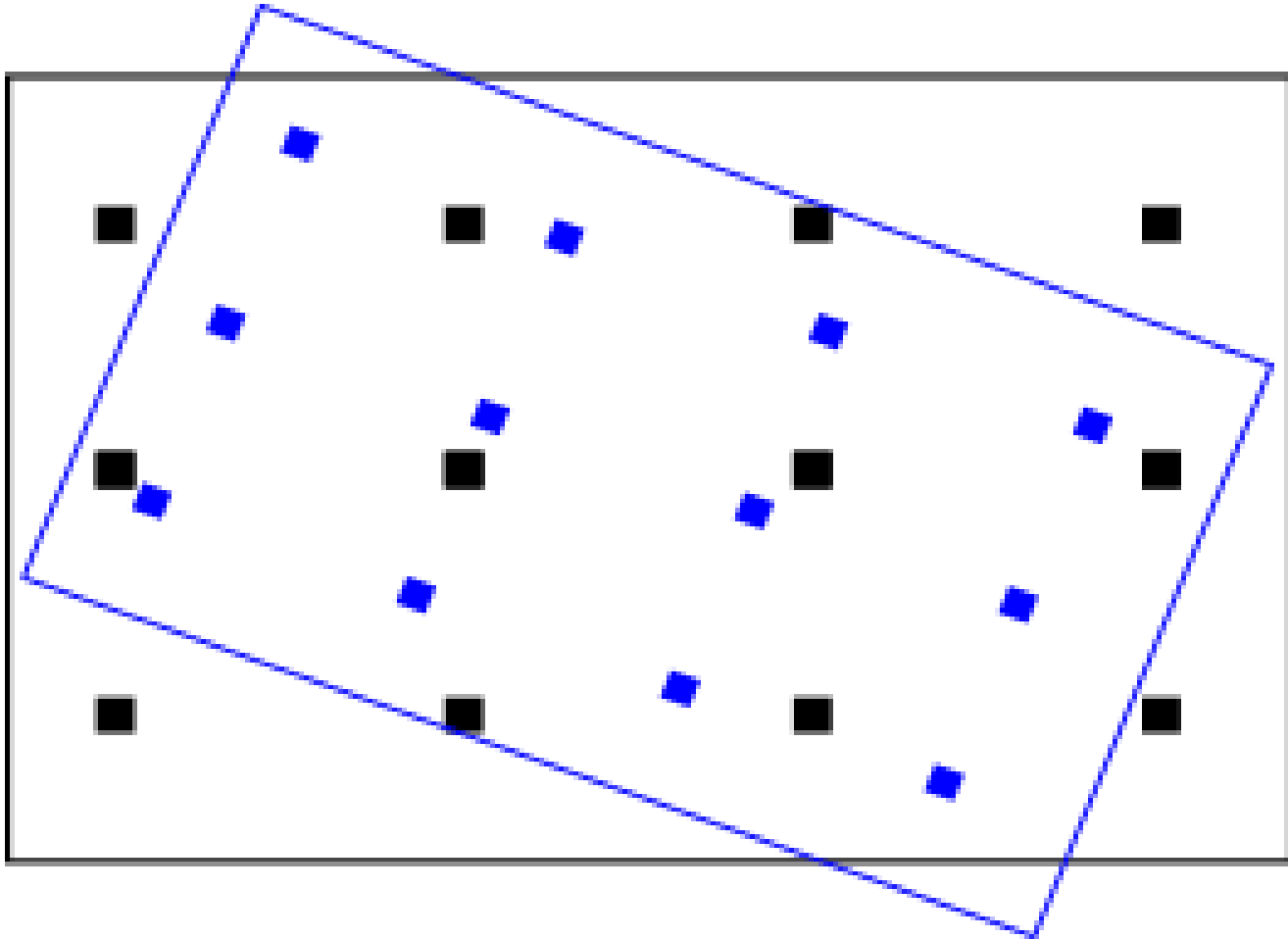


Transforming an image





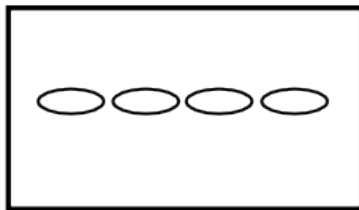
Interpolation



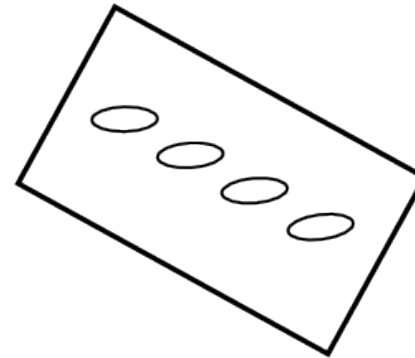
Structure preservation (1)



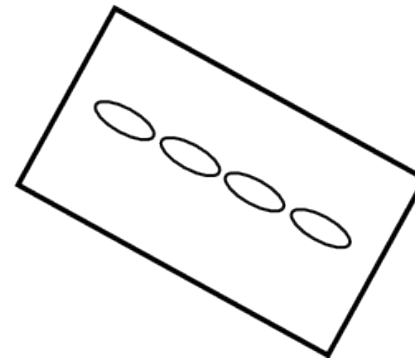
Original Image



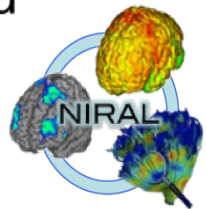
Transformed Image



Structure
not
preserved



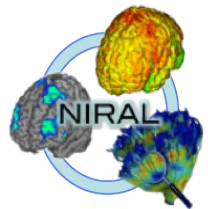
Structure
preserved



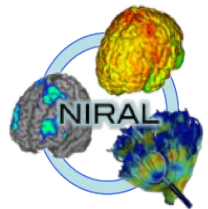
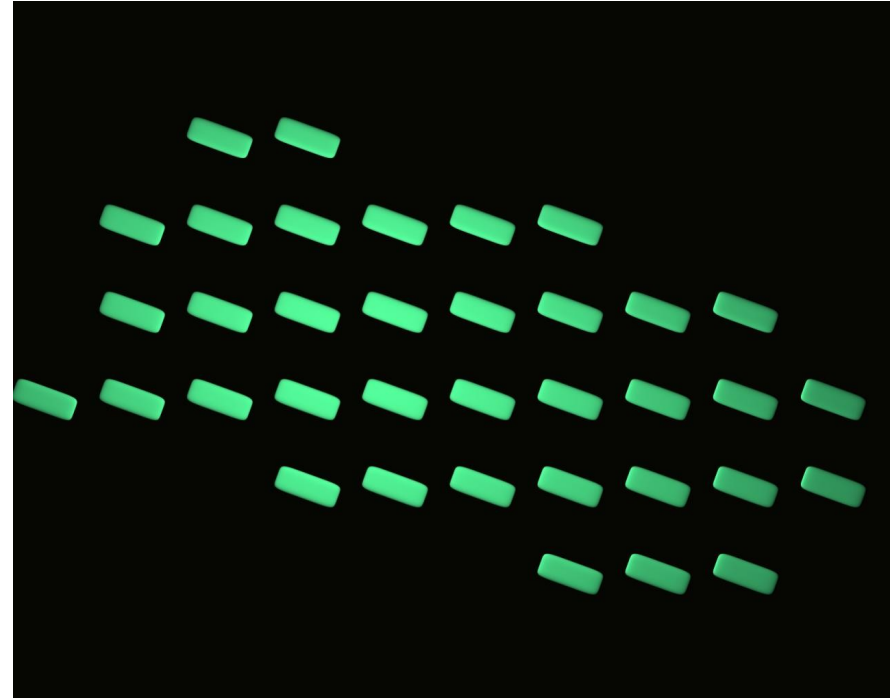
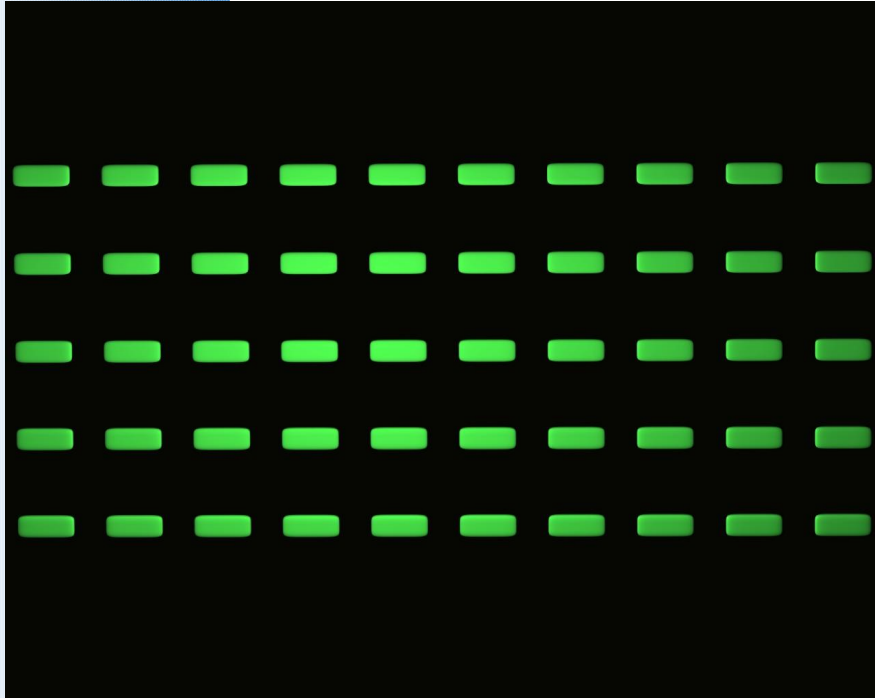
Structure preservation (2)



- A transformation has to be applied to the tensors.
- The transformation should not change the size of the tensors (the tissue's properties are not modified).
- In the case of a rotation, the same transformation is applied to transform the points and to transform the tensors.
- In the case of a more complex transformation, the rotation to apply has to be found.



Rotation



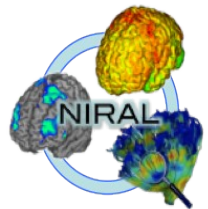


Affine Transformation

2 methods¹:

- Finite Strain
- Preservation of Principal Direction

1 - D.C. Alexander, C. Pierpaoli, P.J. Basser, J.C. Gee. Spatial Transformations of Diffusion Tensor Magnetic Resonance Images, IEEE Transactions on medical imaging, vol. 20, No. 11, November 2001





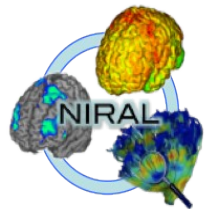
Finite Strain (1)

- The rotation matrix is extracted from the transformation matrix:

$$F=UR$$

$$R=(FF^T)^{-1/2}F$$

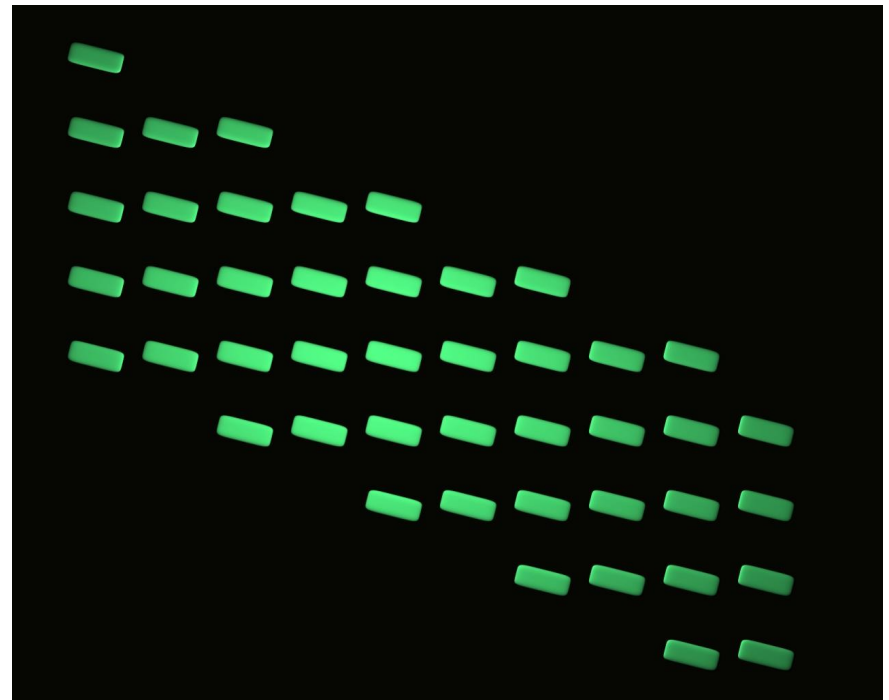
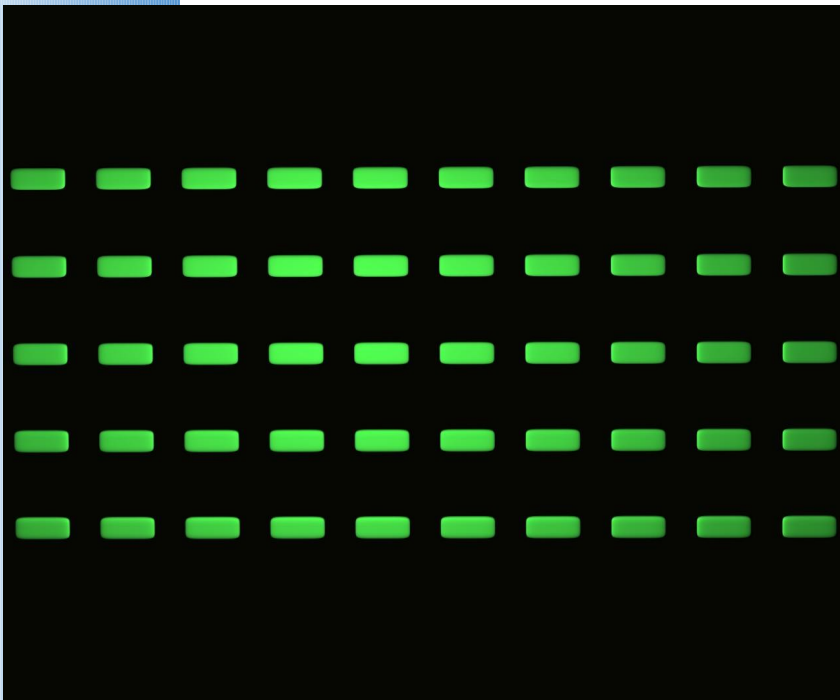
- The matrix is computed only once for the whole image





Finite Strain (2)

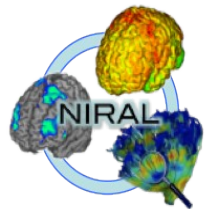
- With some transformations (ie: shearing), the structure is not well preserved



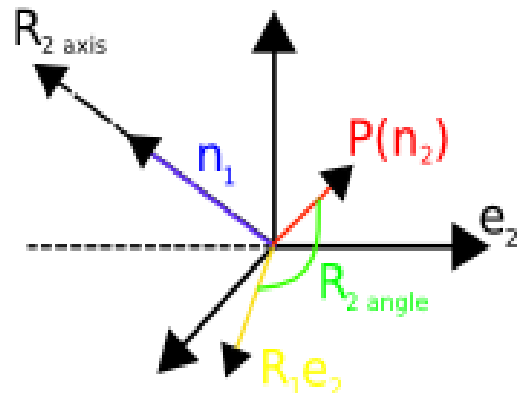
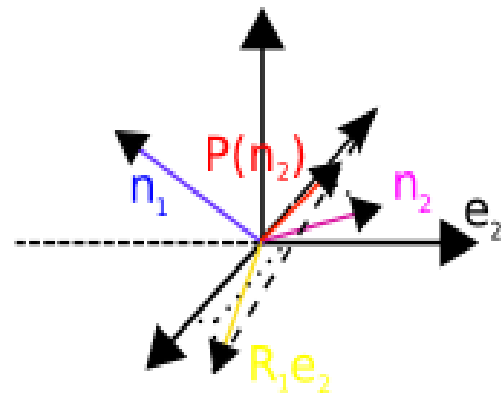
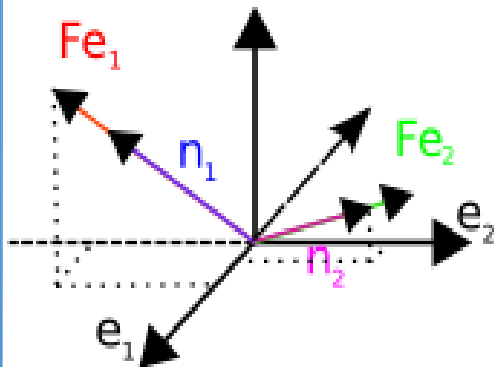
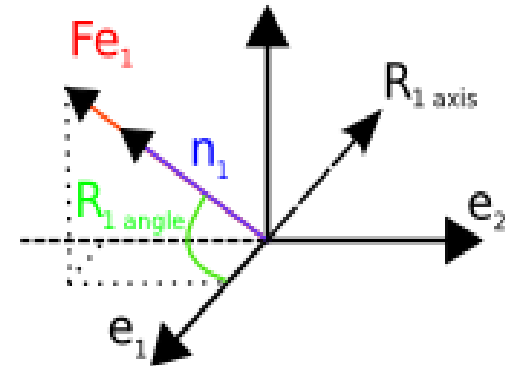
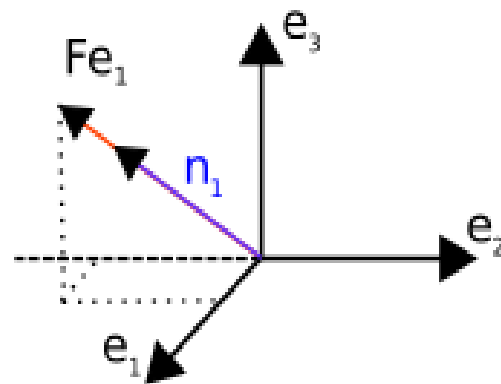
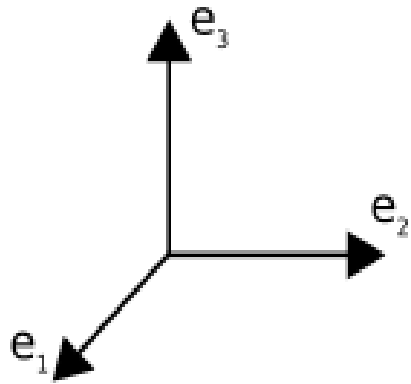
Preservation of Principal Direction (1)



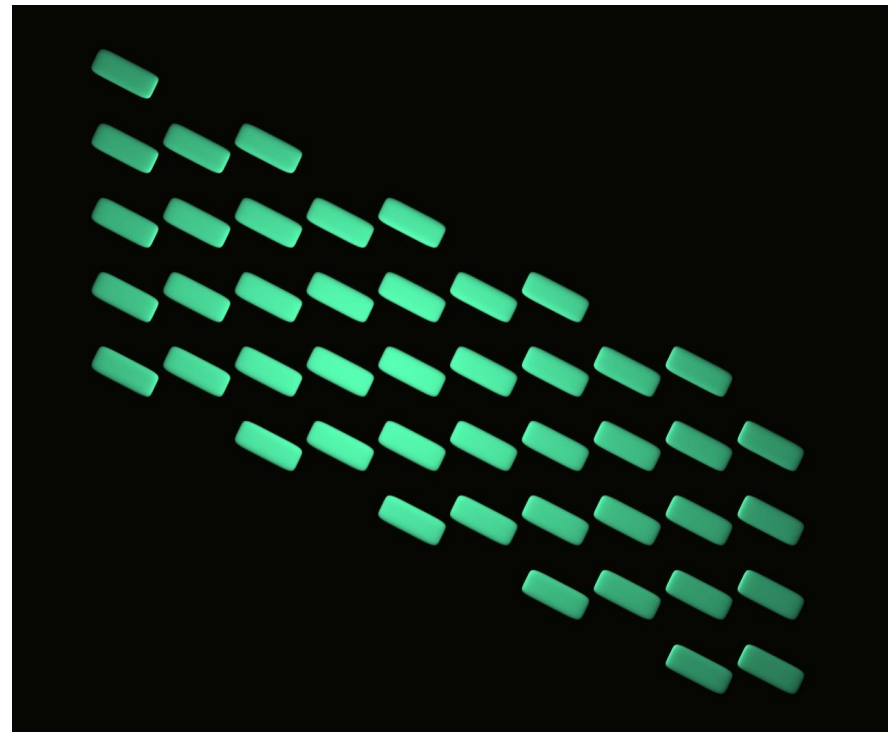
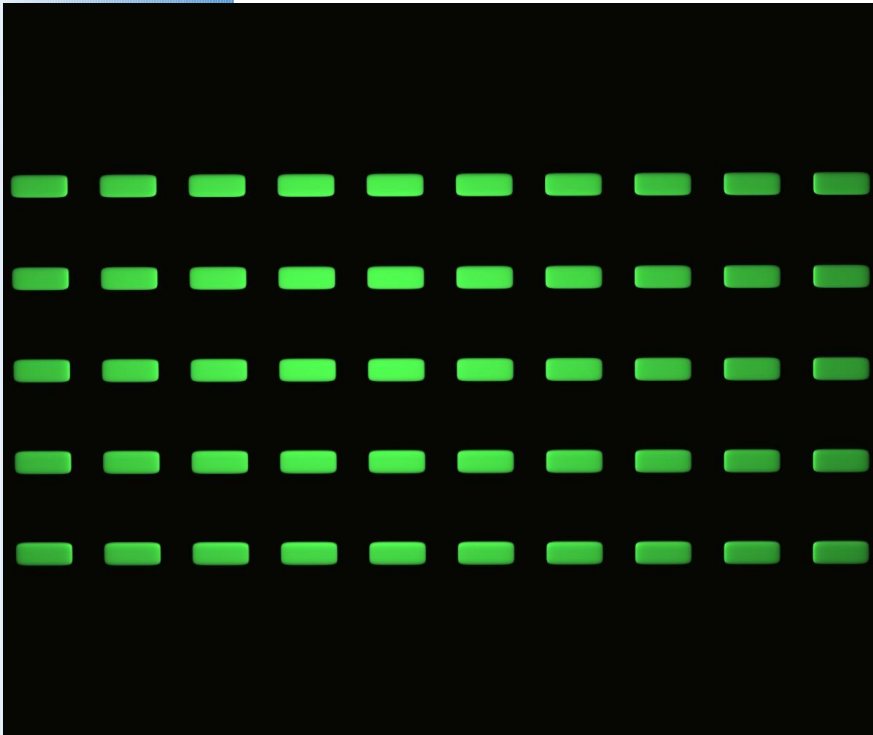
- The transformation applied to a tensor depends on its original orientation.
- The principal direction of a tensor is given by the eigenvector corresponding to its largest eigenvalue.



Preservation of Principal Direction (2)



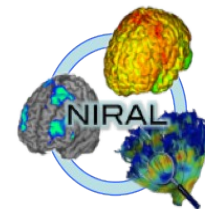
Preservation of Principal Direction (3)



Transformations of higher order



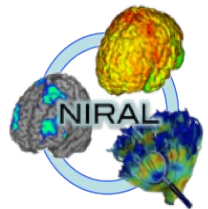
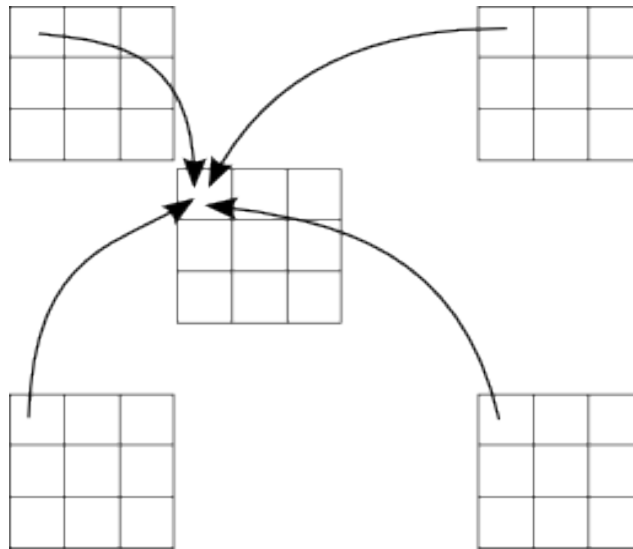
- Any transformation can be expressed as a deformation field $u(x)$ such that at each point of the image $T(x)=x+u(x)$
- If T is an affine transform: $T(x)=Fx+t$
- Deriving both expressions with respect to x gives $F=I+J_u$ where J_u is the Jacobian of u
- This gives a local affine model $F(x)=I+J_u$



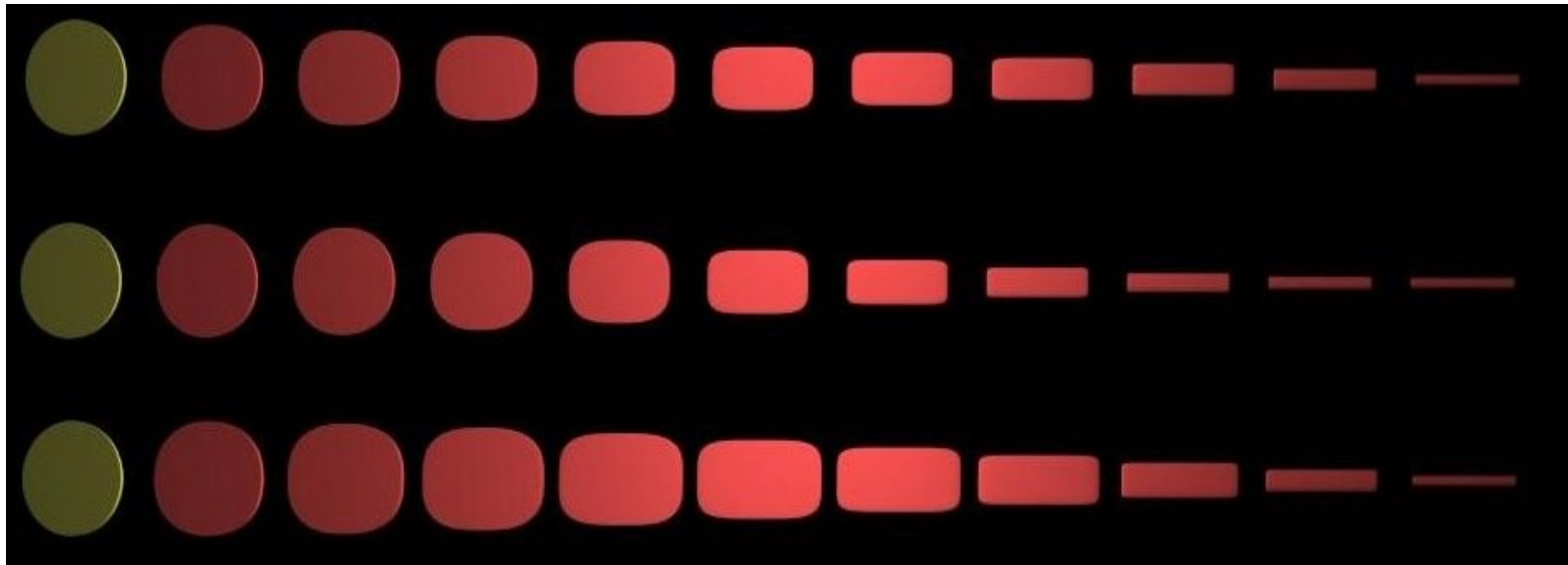


Interpolation

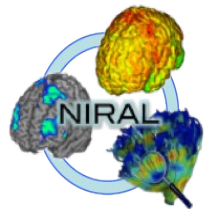
- 2 methods have been implemented:
 - Nearest neighbor
 - Component-wise: each component of the matrix is individually interpolated
- Problem: The resulting matrix does not always belong to the tensor space



Component-wise interpolation



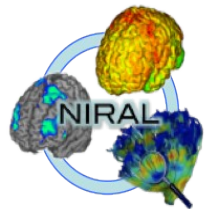
From top to bottom: linear interpolation, B-spline interpolation and Windowed sinc interpolation (Welch)



Tensor Space



- The tensor space is not a vector space but a convex half-cone in the vector space of matrices.
- Some operations are not stable in that space.
- 2 possibilities:
 - To bring back an interpolated matrix into this space, some corrections can be applied.
 - Log-Euclidean Framework



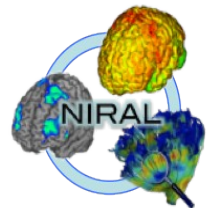


Corrections

- Set negative eigenvalues to zero.
- Set negative eigenvalues to their absolute value.
- Set the matrix representing the tensor to the nearest symmetric positive semi-definite matrix.

X is the nearest symmetric positive semi-definite matrix to A in the Frobenius norm, B is the symmetric part of A and H is the symmetric polar factor of B .

$$\begin{aligned} X &= (B + H)/2 \\ B &= (A + A^T)/2 \\ H &= \sqrt{B^T \cdot B} \end{aligned}$$



Correct computation

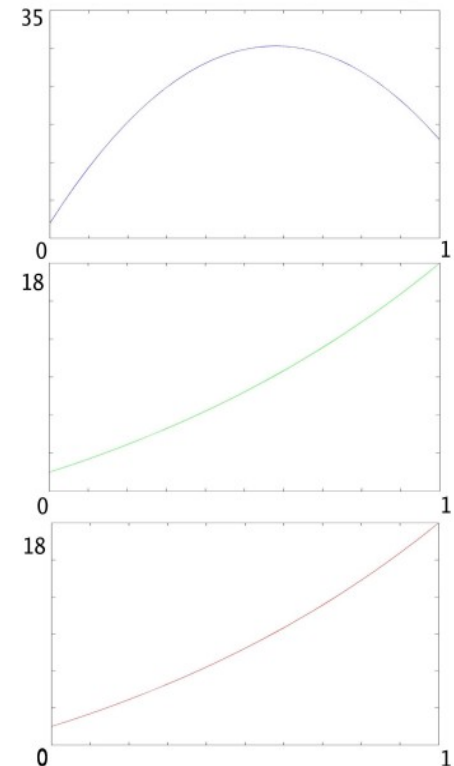
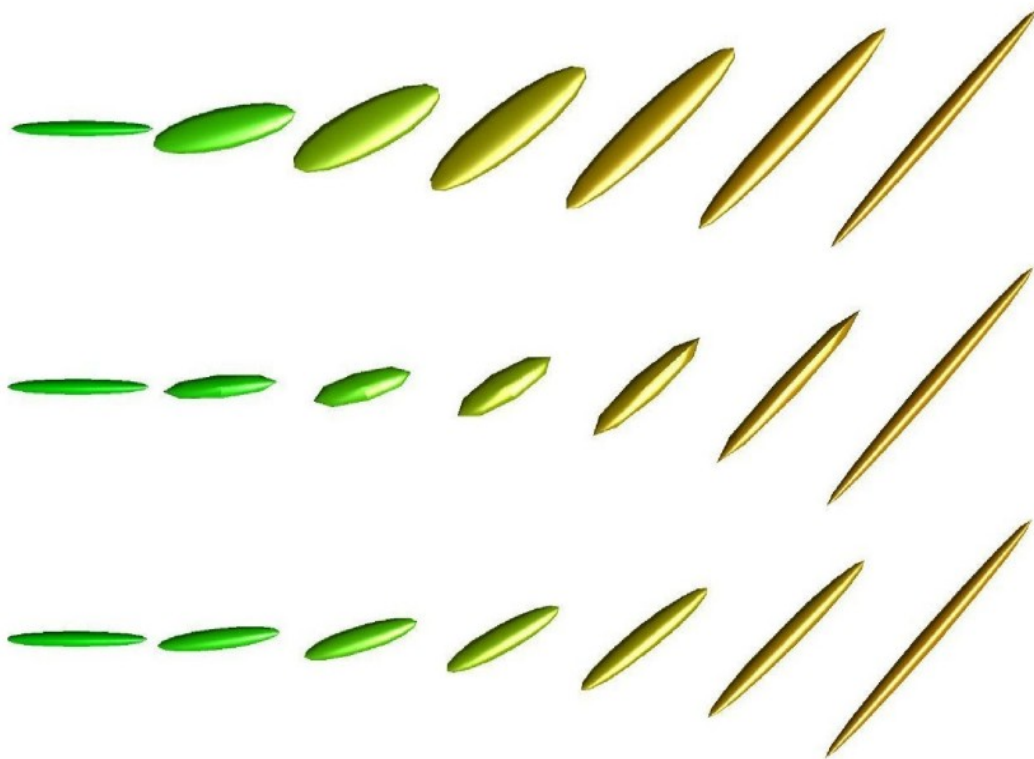


- The Riemannian framework
 - Complex
 - Slow
- The Log-Euclidean framework
 - Compute the logarithm of the tensors
 - Interpolate
 - Compute the exponential of the tensors

Log-Euclidean Framework

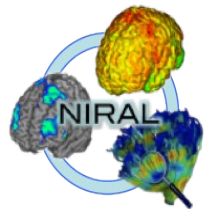
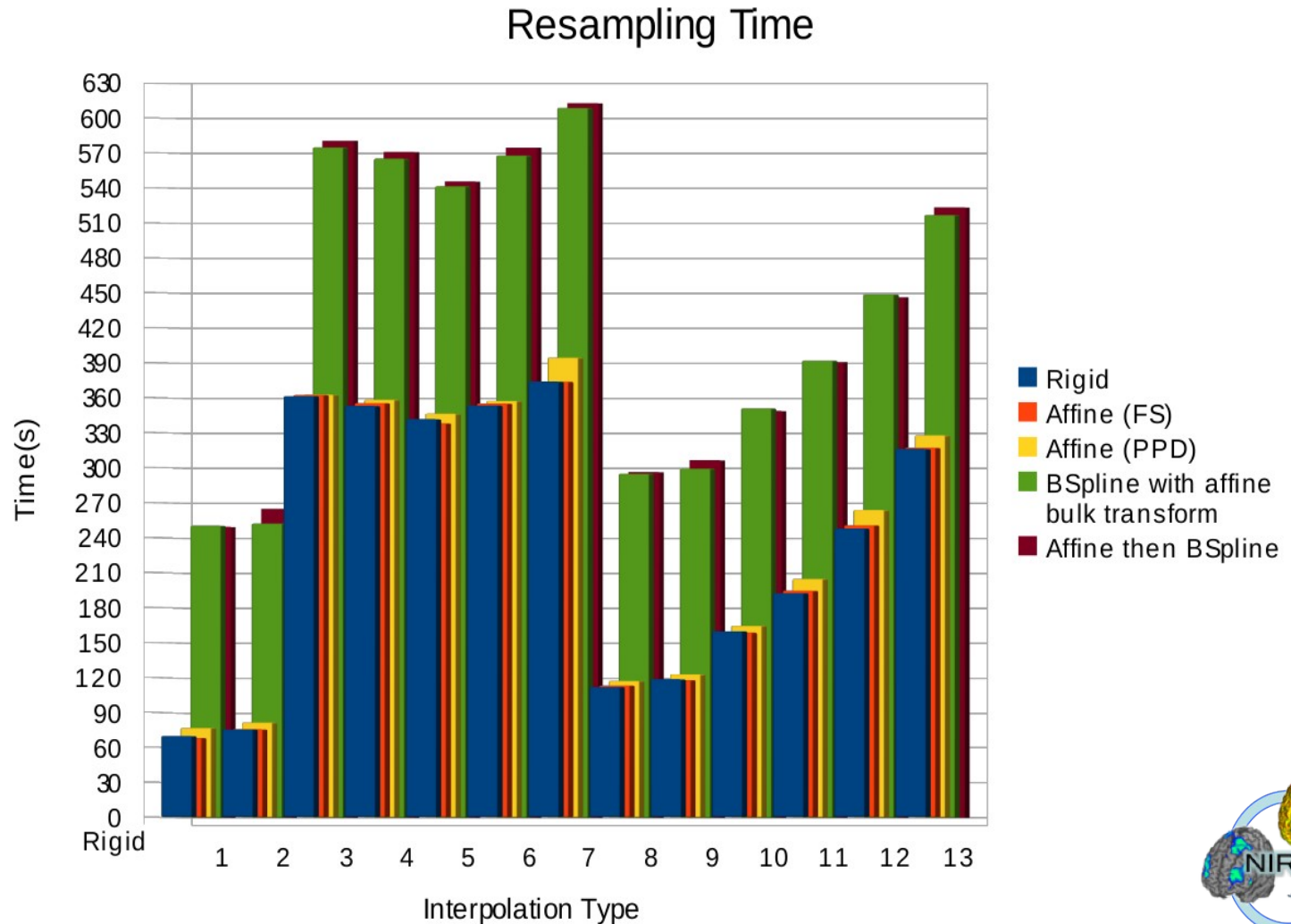


Top to bottom: Linear component-wise interpolation, affine-invariant interpolation, log-Euclidean interpolation



Log-Euclidean Metrics for Fast and Simple Calculus on Diffusion Tensors. Vincent Arsigny, Pierre Fillard, Xavier Pennec, Nicholas Ayache. *Magnetic Resonance in Medicine*, Vol. 56, No. 2. (2006), pp. 411-421

Processing time

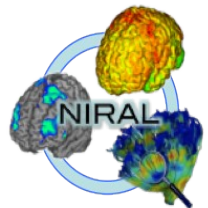


Memory usage

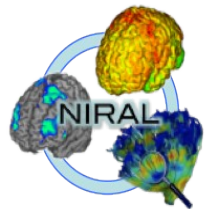
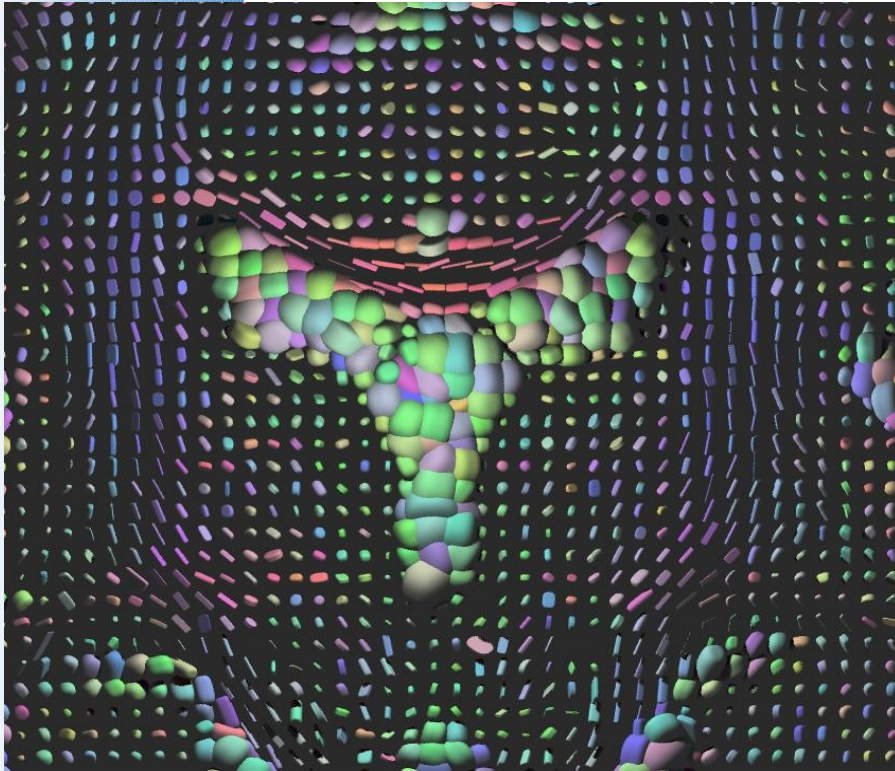


| Images | |
|-----------------------------------|---|
| Input image | 768MB |
| Output image | 768MB |
| Interpolators | |
| Nearest Neighborhood | No additional memory used |
| Linear, BSpline and Windowed Sinc | 768MB (input image size) to separate the components of the tensors into different images |
| BSpline | Additional 768MB (input image size) for the <code>itk::BSplineDecompositionImageFilter</code> used in the BSpline interpolator. |
| Deformations | |
| Deformation field | 768MB |
| Other transformations | Small amount of memory used |

Input image: 512x256x256, float values



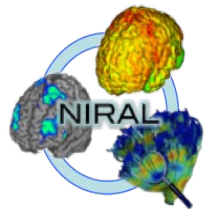
Some results: after a 45 degrees rotation



Conclusion



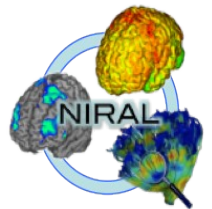
- New interpolation algorithm could be created
- Implemented as a module in Slicer3
- Submission of an Insight Journal paper



Acknowledgements



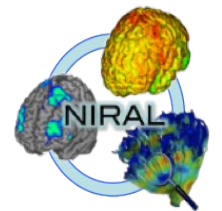
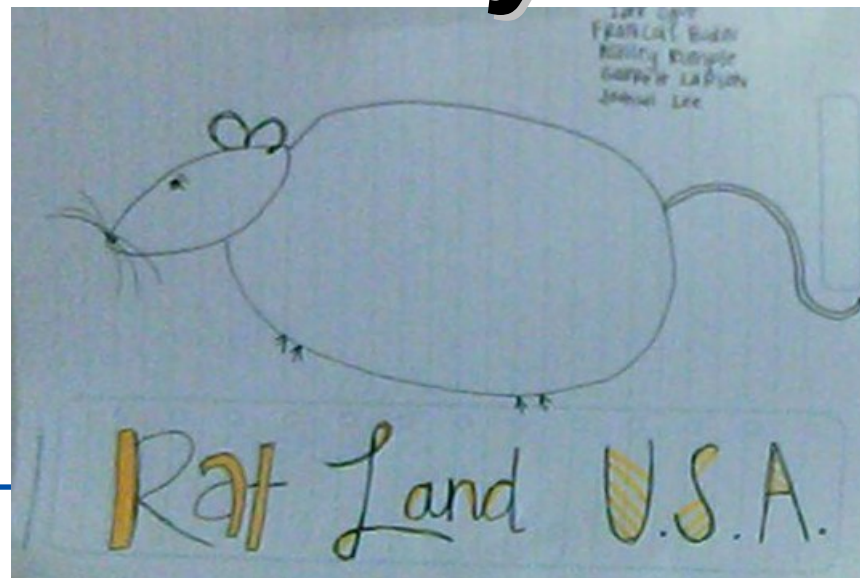
- Martin Styner, Ph.D, UNC
- Ipek Oguz, Ph.D., UNC
- Sylvain Bouix, Ph.D., BWH
- Martha Shenton, Ph.D., BWH





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Thank you!



Lab logo – courtesy Ashley Rumple